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Can shoulder range of movement be measured accurately using the Microsoft Kinect sensor plus Medical Interactive Recovery Assistant (MIRA) software?

James D. Wilson, FRCS(TrOrth)^{a,*}, Jennifer Khan-Perez, MBBS^b, Dominic Marley, MBBS^c, Susan Buttress, MPhil^d, Michael Walton, FRCS(TrOrth)^e, Baihua Li, PhD^f, Bibhas Roy, FRCS(TrOrth)^g

^aTrauma and Orthopaedics Department, Bolton National Health Service Foundation Trust, Manchester, UK

^bMedical School, Manchester University, Manchester, UK

^cTrauma and Orthopaedics Training Rotation, North West Deanery, Manchester, UK

^dSchool of Health Sciences, Salford University, Salford, UK

^eTrauma and Orthopaedics Department, Wrightington Wigan and Leigh National Health Service Foundation Trust, Wigan, UK

^fComputer Science Department, Loughborough University, Loughborough, UK

^gTrauma and Orthopaedics Department, Central Manchester University, Hospitals National Health Service Foundation Trust, Manchester UK

Background:: This study compared the accuracy of measuring shoulder range of movement (ROM) with a simple laptop-sensor combination vs. trained observers (shoulder physiotherapists and shoulder surgeons) using motion capture (MoCap) laboratory equipment as the gold standard.

Methods: The Microsoft Kinect sensor (Microsoft Corp., Redmond, WA, USA) tracks 3-dimensional human motion. Ordinarily used with an Xbox (Microsoft Corp.) video game console, Medical Interactive Recovery Assistant (MIRA) software (MIRA Rehab Ltd., London, UK) allows this small sensor to measure shoulder movement with a standard computer. Shoulder movements of 49 healthy volunteers were simultaneously measured by trained observers, MoCap, and the MIRA device. Internal rotation was assessed with the shoulder abducted 90° and external rotation with the shoulder adducted. Visual estimation and MIRA measurements were compared with gold standard MoCap measurements for agreement using Bland-Altman methods. **Results:** There were 1670 measurements analyzed. The MIRA evaluations of all 4 cardinal shoulder movements were significantly more precise, with narrower limits of agreement, than the measurements of trained observers. MIRA achieved $\pm 11^\circ$ (95% confidence interval [CI], 8.7°-12.6°) for forward flexion vs. $\pm 16^\circ$ (95% CI, 14.6°-17.6°) by trained observers. For abduction, MIRA showed $\pm 11^\circ$ (95% CI, 8.7°-12.8°) against

Accurate measurement of shoulder range of movement (ROM) is an extremely important element of assessing shoulder pathology. Restriction of shoulder movement limits function. Identifying impaired ROM aids diagnosis and evaluation of severity for common conditions such as frozen shoulder, rotator cuff deficiency, and subacromial impingement. Repeat measurement can help to track a patient's recovery or response to treatment.^{3,13}

Various methods of measurement are used to help manage shoulder rehabilitation, including the traditional goniometer, questionnaires,¹³ camcorders, electromagnetic sensors,^{15,16} and visual estimation.¹² An accurate, automated process may be more efficient and objective compared with traditional assessments.^{12,14} The use of remote sensor technology provides several advantages over conventional modes of measurement. It delivers increased capacity for quantification of motor performance and real-time feedback enhancing patient motivation.¹⁰

The Kinect sensor (Microsoft Corp., Redmond, WA, USA) was developed as an add-on for the Xbox 360 video game console (Microsoft Corp.). It allows users to interact with the gaming system by tracking body movement in 3 dimensions (3D). The key to the 3-D movement recognition is the sensor's depth camera, which uses an infrared (IR) laser projector that generates a speckle pattern and an IR camera that detects the reflections from objects. The Kinect is able to create a 3-D map of these objects by measuring deformations in the reference speckle pattern.⁷ The Kinect sensor can be paired with a standard notebook or desktop computer and software developed to measure and track body movements; for example, as part of an in-home shoulder rehabilitation program.

The current gold standard method of measuring body movement is by using motion capture (MoCap) technology such as the Vicon (Vicon Motion Systems Ltd., Oxford, UK) marker-tracking system. It incorporates multiple high-resolution cameras and makes use of IR reflective markers to achieve millimeter resolution of 3-D spatial displacements at greater than 100 frames per second.^{7,11} Conversely, clinical assessment and rehabilitation of patients with shoulder pathology is routinely performed by trained observers who visually assess shoulder movement without the aid of sensors or MoCap technology.

This study assessed the accuracy of the Kinect sensor paired with the software developed by Medical Interactive Recovery Assistant (MIRA; MIRA Rehab Ltd., London, UK). Therefore, the level of agreement between MoCap and the

Kinect + MIRA system was compared with the level of agreement between MoCap and the visual estimation of trained observers.

Materials and methods

The investigation was conducted in the dedicated MoCap laboratory at the Institute for Biomedical Research into Human Movement. This MoCap laboratory in Manchester University uses a Vicon system consisting of 10 high-resolution cameras fitted with IR optical filters and an array of IR light-emitting diodes for illumination. The cameras were calibrated before the MoCap session. The calibration accuracy achieved was 0.01 mm. Forty-nine healthy individuals consented to participate. Reflective markers were applied to the participants in a standardized pattern, based on surface anatomic locations (plug-in-gait model upper limbs and thorax; Fig. 1). Using the 3-D locations of these markers recorded by the system in real-time, the Vicon software calculated joint centers and composite shoulder movement relative to the thorax (scapula-thoracic and glenohumeral motions combined).

The Kinect sensor was set up within the MoCap laboratory to facilitate simultaneous measurements. The sensor was placed 1.5 m above the floor on a tripod, 2 to 3 m from the participant (Fig. 2). A Universal Serial Bus 2.0 port was used to connect the Kinect sensor

Figure 1 Positions of infrared reflective markers. The 4 additional markers without labels are right and left elbow A and right and left anterior superior iliac spine. CLAV, medial clavicle; LELB, left elbow B; LSHO, left shoulder; LUPA, left upper arm; LWRA, left wrist A; LWRB, left wrist B; RELB, right elbow B; RSHO, right shoulder; RUPA, right upper arm; RWRA, right wrist A; RWRB, right wrist B; STRN, sternum.

Figure 2 Study set-up showing motion capture cameras, Medical Interactive Recovery Assistant (MIRA) software (MIRA Rehab Ltd., London, UK)/Kinect (Microsoft Corp., Redmond, WA, USA) sensor, and trained observers.

Figure 3 Screen shot of Medical Interactive Recovery Assistant (MIRA) software (MIRA Rehab Ltd., London, UK) displaying measured abduction angle using the Kinect (Microsoft Corp., Redmond, WA, USA) sensor. (The screen is set up to act as a mirror for a more intuitive user experience, hence the apparent left-right discrepancy).

to a Lenovo (Beijing, China) laptop with a Windows 7 (Microsoft Corp.), 64-bit operating system, 8 GB of random access memory, and a 2.3-GHz Intel i7 (Intel Corp., Santa Clara, CA, USA) pro-cessor. MIRA software was used to process the Kinect data. This was achieved using the Microsoft Kinect Software Development Kit (SDK) 1.8 for Windows and the ROM measurement tool that is part of the MIRA 1.3 platform software installed on the laptop. MIRA calculated the 3D angle of composite shoulder movement and displayed the result in real time (Fig. 3).

In addition to the Vicon system and the Kinect + MIRA pairing, trained observers also recorded their visual assessment of the angle of shoulder movement. These observers comprised 1 consultant orthopedic surgeon, 2 orthopedic specialty trainee registrars, 3 upper limb specialist physiotherapists, and 1 medical student who had received specific training in shoulder ROM assessment for this project. As in a standard clinical setting, the observers were allowed to move around the participants to view them from different positions while estimating the shoulder movement angles, without additional equipment such as

goniometers. This was to emulate routine clinical practice and to allow multiple simultaneous observations to be made.

The participants were asked to perform each of the 4 cardinal shoulder movements: abduction, forward flexion, and internal and external rotation. External rotations were performed with the shoulder adducted. Internal rotation was performed with the shoulder abducted at 90°. This abducted position was used so that the participant's trunk did not act as a block to full internal rotation. Each movement was then held in a static position to allow simultaneous measurement by the Kinect + MIRA system, the MoCap, and the trained observers. To assess agreement across the full spread of possible measurements, the participants were asked to move their shoulder to the full extent of its range and then were asked to repeat the movement to a point short of full range. This second position was chosen by the participant to help generate a pseudorandom spread of different shoulder positions. The measurements were performed for both shoulders of each participant.

The trained observers were blinded to the measurements of the other observers and of the Kinect + MIRA system. The data from the MoCap system required extensive processing, which was performed over several days after completion of the study. This analysis allowed calculation of the movement angles. This was done in isolation from the Kinect + MIRA operator and the group of trained observers. Therefore, there was no possibility of the measurements from the trained observers or the Kinect + MIRA system being biased or influenced by the measurements the MoCap system recorded.

Statistical analysis

Agreements between the gold standard (MoCap) and the other 2 methods of measurement (Kinect + MIRA and estimation by trained observers) were analyzed as recommended by Bland and Altman.^{1,2} This comprised calculating the difference from the MoCap measurement for every Kinect + MIRA measurement and each trained observer measurement. The spread of these differences was then tested for normality using the Shapiro-Wilk calculation. Correlations were assessed using the Pearson test or the Spearman test if a normal distribution was not present. Scatter plots of these correlations were then generated. Agreement between the measurements methods were demonstrated using Bland-Altman plots. The limits of agreement (LOA) were calculated, and the 95% confidence intervals (CIs) of the LOA were also calculated. These analyses were performed using IBM SPSS Statistics 22 software (IBM, Armonk, NY, USA).

Results

There were 1670 measurements available for analysis from the observers, MoCap, and MIRA + Kinect systems. The analysis had to exclude 49 measurements from the MoCap system because interference with IR reflections prevented calculation of the angle of shoulder movement. However, only 1 MIRA + Kinect measurement was identified as an outlier requiring exclusion, and no measurements recorded by the trained observers required exclusion.

Correlations between the MoCap measurements and the other modes of measurement are reported in Table I. Scatter plots were also produced for comparison of the correlations with MoCap measurements (Fig. 4). These charts demonstrate

Table I Correlation coefficients with motion capture for the cardinal shoulder movements

Variable	Correlation coefficient of motion capture	
	With trained observers	With MIRA/Kinect
Forward flexion	0.928 ^{*,†}	0.993 ^{*,‡} (0.949)
Abduction	0.984 ^{*,†}	0.991 ^{*,‡} (0.967)
External rotation	0.865 ^{*,†}	0.961 ^{*,‡}
Internal rotation	0.922 ^{*,†}	0.970 ^{*,‡}

Kinect, Microsoft Corp., Redmond, WA, USA; *MIRA*, Medical Interactive Recovery Assistant, MIRA Rehab Ltd., London, UK.

* Correlation significant at the .01 level (2-tailed).

† Spearman test used as differences from the motion capture result did not follow a normal distribution (Shapiro-Wilk test <.05).

‡ Pearson test used as differences from the motion capture result followed a normal distribution (Shapiro-Wilk test >.05). The Spearman test is also reported in parentheses for comparison.

Table II Limits of agreement of the 2 measurement methods with motion capture for the cardinal shoulder movements

Variable	Trained observer		MIRA/Kinect	
	Limits of agreement (°)	95% CI (°)	Limits of agreement (°)	95% CI (°)
Forward flexion	16	14.6-17.6	11	8.7-12.6
Abduction	15	13.4-16.2	11	8.7-12.8
External rotation	21	18.7-22.6	10	8.1-11.9
Internal rotation	18	16.0-19.3	9	7.2-10.4

a much closer correlation with the MoCap measurements for the MIRA + Kinect system compared with the trained observer measurements.

To analyze the different measurement techniques further, the agreement was assessed using Bland-Altman plots (Fig. 5) and calculation of the LOA.^{1,2} These charts indicate the mean difference from the MoCap measurements as the solid black line, with the 95% CI of this value shown by the solid red lines above and below it. The LOA are represented by the dotted black lines above and below the mean. The 95% CIs of these values were also calculated and are shown as the dotted green lines. The LOA and their 95% CIs are pre-sented in Table II for further clarity.

These Bland-Altman charts show that for each of the cardinal shoulder movements, the MIRA + Kinect system has a narrower spread of plots compared with the results from the trained observers. The calculated LOA show that the MIRA + Kinect has closer agreement to the MoCap than the trained observers. Furthermore, the 95% CIs of these values do not overlap, indicating that the superior agreement that has been found is statistically

significant. The values pre-sented in Table II show how closely each measurement method agrees with the gold standard MoCap measurement. For example, 95% of the measurements performed by trained observers for forward flexion should lie within $\pm 16^\circ$ of the MoCap measurement. However, the MIRA + Kinect system agrees more closely with 95% of measurements, lying within $\pm 11^\circ$.

Discussion

The power to measure and monitor shoulder movement using a portable and inexpensive sensor-based system brings potential benefits to research and clinical applications across a wide range of patient populations.^{5,8} We compared both measurement techniques to the Vicon MoCap system because this is considered the gold standard for measurement accuracy. The MIRA + Kinect system carries benefits and drawbacks compared with other practical aspects of MoCap. Beyond the benefits of lower cost and portability, the MIRA + Kinect system does not require markers placed on the skin, which avoids lengthy set up time, potentially indelicate body exposure, and problems with inaccurate marker position.⁵

Vicon MoCap technology is vulnerable to interference with data collection caused by reflections from extraneous objects within the field of view or loss of signal from the IR reflective markers. The trained observers were asked to remove jewelry that could reflect IR and to avoid standing in positions that would block the line-of-sight of the MoCap cameras. However, despite these procedures and despite conducting the study in a dedicated MoCap laboratory with 10 high-resolution cameras, 49 measurements (13%) were still lost to analysis because interference precluded calculation of the shoulder movement angles. This demonstrates that regardless of the superior accuracy of the Vicon MoCap system, it faces limitations even when conditions are optimized and would not be a practical technology to apply within a clinical or home setting with limited space, multiple background objects, and people moving around.⁷

In contrast to this, we found that the MIRA + Kinect system would be more appropriate for use in a clinical or home-based rehabilitation role because it only produced 1 outlying data point (0.3%) necessitating exclusion. It also uses sensors specifically designed to work within the home environment.⁷ However, it is important to note that the ability of the Vicon MoCap system to differentiate between scapulothoracic and glenohumeral components of shoulder movement is not emulated by the MIRA + Kinect system because only composite shoulder movement can be measured.

This study has demonstrated that the MIRA + Kinect system has better agreement with gold standard measurement compared with estimation by trained observers. However, there are other aspects to consider. Additional benefits of the system over trained observers is the objective nature of the sensor technology. The system can provide unbiased measurement for comparison between groups or before and after an intervention for the same individuals. Furthermore, although the system does involve a laptop and a Kinect sensor, its operation does

Figure 4 Scatter plots of measurement methods against motion capture (*MoCap*) for cardinal shoulder movements. *MIRA*, Medical Interactive Recovery Assistant, MIRA Rehab Ltd., London, UK; *Kinect*, Microsoft Corp., Redmond, WA, USA.

Figure 5 Bland-Altman Plots of measurement methods against motion capture (*MoCap*) for cardinal shoulder movements. The *solid black line* is the mean difference from the MoCap measurements, and the *solid red lines* indicate the 95% confidence interval of this value. The *dotted black lines* show the limits of agreement, with the *dotted green lines* indicating the 95% confidence intervals.

not require a trained professional such as a specialist physio-therapist or orthopedic surgeon. Individuals can operate the system without supervision by following on-screen directions.

The utility of the Kinect sensor has been evaluated for joint position¹⁷ movement analysis in postural control and gait retraining,^{4,6} use in people with Parkinson disease,⁹ and authors have concluded that the sensor is useful as a means of measuring gross body movements and ergonomic assessments in “the field.”⁷ Xu and McGorry¹⁷ found that the Kinect did not accurately identify joint centers, particularly for lower limb joints, but did comment that joint angle measurement may be of greater interest for occupational tasks than pure joint location.

Other authors have also assessed use of a Kinect sensor to specifically measure shoulder movement. Huber et al¹⁰ compared the Kinect sensor to goniometer measurement and to electromagnetic motion tracking sensors. They found increased levels of bias and broader limits of agreement. The MIRA software used with the Kinect sensor in our study has undergone several cycles of refinement to optimize the positioning of the participants and the movements they perform, which may account for the different conclusion. In addition, we compared the MIRA + Kinect system with the performance of trained observers, emulating routine clinical practice, rather than taking 5° as an arbitrary target value.

Use of a sensor-based technology to measure shoulder movement has clear utility in providing objective data for re-search applications. It is unlikely to replace clinician observation to estimate shoulder ROM during routine clinical assessment, but it opens the possibilities of using this system to enhance rehabilitation protocols. Patients can be encouraged to engage with their shoulder exercise program by harnessing the principles of gamification within tailored “Exergames.”⁹ Having good evidence that this technology can accurately track shoulder movement is a necessity before clinicians should consider its implementation.

Other novel technologies, such as wearable sensors, are being developed, also with the aim of accurately plotting body movements and using them for shoulder rehabilitation.¹² Furthermore, an updated Kinect sensor (Kinect 2) offers increased sensitivity and the potential for motion analysis of smaller joints.^{5,17}

We acknowledge that our study has several limitations. The participants were all asked to wear close-fitting garments to facilitate IR marker positioning. This is also beneficial for the Kinect sensor. We have not compared the different measurement methods for situations where loose or baggy clothing is being worn. Clinical examination is normally performed with appropriate exposure of the limb, but if the sensor is being used in a home setting, a participant may not remove baggy garments for the assessment.

The measurement of internal rotation was performed with the participant abducting the shoulder to 90°. This position was used so that the forearm can move freely, without contacting the participant’s abdomen. This position of abduction may be difficult to reach for some individuals with shoulder pathology.

Performing Vicon and MIRA + Kinect measurements simultaneously meant that the presence of the IR markers could

distort the 3-D model generated by the IR Kinect sensor. However, we found the model had good agreement with the Vicon system, and other authors have found this effect to be minimal.⁵

The participants did not have shoulder pathology and, therefore, do not represent the population that would be using such a system. This did, however, allow testing across the full range of possible shoulder movements, unconstrained by pain or stiffness. Our measurements were also taken with the participants in a static pose. This was to facilitate simultaneous measurement by the MoCap, MIRA + Kinect, and the trained observers. Therefore, our results may not be applicable to dynamic shoulder movements, and further validation of this aspect may be required.

Conclusion

MIRA software paired with a Kinect sensor measures all cardinal shoulder movements with significantly closer agreement to Vicon MoCap than trained observer measurements. Therefore, use of this system to measure shoulder movement during shoulder assessment and re-habilitation would be acceptable. In addition, this technology may allow precise shoulder ROM measurement outside the clinic setting.

Disclaimer

Bibhas Roy has been a clinical advisor to MIRA Rehab since 2013. This has helped shape the exergames development by providing clinical context. He has not received any direct financial benefit from MIRA Rehab and has not invested money in the company but does hold share options in the company. All of the other authors, their immediate families, and any research foundations with which they are affiliated have not received any financial payments or other benefits from any commercial entity related to the subject of this article.

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References

1. Bland JM, Altman DG. Statistical methods for assessing agreement between two methods of clinical measurement. *Lancet* 1986;1:307-10.
2. Bland JM, Altman DG. Measuring agreement in method comparison studies. *Stat Methods Med Res* 1999;8:135-60.
3. Bunker T. (ii) Frozen shoulder. *Orthop Trauma* 2011;25:11-8. <http://dx.doi.org/10.1016/j.mporth.2011.01.007>

4. Clark RA, Pua YH, Bryant AL, Hunt MA. Validity of the Microsoft Kinect for providing lateral trunk lean feedback during gait retraining. *Gait Posture* 2013;38:1064-6. <http://dx.doi.org/10.1016/j.gaitpost.2013.03.029>
5. Clark RA, Pua YH, Fortin K, Ritchie C, Webster KE, Denchey L, et al. Validity of the Microsoft Kinect for assessment of postural control. *Gait Posture* 2012;36:372-7. <http://dx.doi.org/10.1016/j.gaitpost.2012.03.033>
6. Clark RA, Pua YH, Oliveira CC, Bower KJ, Thilarajah S, McGaw R, et al. Reliability and concurrent validity of the Microsoft Xbox One Kinect for assessment of standing balance and postural control. *Gait Posture* 2015;42:210-3. <http://dx.doi.org/10.1016/j.gaitpost.2015.03.005>
7. Dutta T. Evaluation of the Kinect sensor for 3-D kinematic measurement in the workplace. *Appl Ergon* 2012;43:645-9.
8. Fernández-Baena A, Susin A, Lligadas X. Biomechanical validation of upper-body and lower-body joint movements of kinect motion capture data for rehabilitation treatments. Presented at the 2012 Fourth International Conference on Intelligent Networking and Collaborative Systems, Bucharest, Romania, Sept 19-21, 2012. IEEE. 2012. p. 656-61. <http://dx.doi.org/10.1109/INCoS.2012.66>
9. Galna B, Barry G, Jackson D, Mhiripiri D, Olivier P, Rochester L. Accuracy of the Microsoft Kinect sensor for measuring movement in people with Parkinson's disease. *Gait Posture* 2014;39:1062-8. <http://dx.doi.org/10.1016/j.gaitpost.2014.01.008>
10. Huber ME, Seitz AL, Leeser M, Sternad D. Validity and reliability of Kinect skeleton for measuring shoulder joint angles: a feasibility study. *Physiotherapy* 2015;101:389-93. <http://dx.doi.org/10.1016/j.physio.2015.02.002>
11. Leightley D, Darby J, Li B, McPhee JS, Yap MH. Human activity recognition for physical rehabilitation. Presented at the 2013 IEEE International Conference Systems, Man, and Cybernetics-SMC Manchester, UK, Oct 13-16 2013. <http://dx.doi.org/10.1109/SMC.2013.51>
12. Lin HC, Chiang SY, Lee K, Kan YC. An activity recognition model using inertial sensor nodes in a wireless sensor network for frozen shoulder rehabilitation exercises. *Sensors (Basel)* 2015;15:2181-204. <http://dx.doi.org/10.3390/s150102181>
13. Mao CY, Jaw WC, Cheng HC. Frozen shoulder: correlation between the response to physical therapy and follow-up shoulder arthrography. *Arch Phys Med Rehabil* 1997;78:857-9.
14. Maund E, Craig D, Suekarran S, Neilson AR, Wright K, Brealey S, et al. Management of frozen shoulder: a systematic review and cost-effectiveness analysis. *Health Technol Assess* 2012;16:<http://dx.doi.org/10.3310/hta16110>
15. Rundquist PJ, Anderson DD, Guanche CA, Ludewig PM. Shoulder kinematics in subjects with frozen shoulder. *Arch Phys Med Rehabil* 2003;84:1473-9. [http://dx.doi.org/10.1016/S0003-9993\(03\)00359-9](http://dx.doi.org/10.1016/S0003-9993(03)00359-9)
16. Walther M, Werner A, Stahlschmidt T, Woelfel R, Gohlke F. The subacromial impingement syndrome of the shoulder treated by conventional physiotherapy, self-training, and a shoulder brace: results of a prospective, randomized study. *J Shoulder Elbow Surg* 2004;13:417-23.
17. Xu X, McGorry RW. The validity of the first and second generation Microsoft Kinect™ for identifying joint center locations during static postures. *Appl Ergon* 2015;49:47-54. <http://dx.doi.org/10.1016/j.apergo.2015.01.005>